

(19)

Europäisches Patentamt

European Patent Office

Office européen des brevets



(11)

EP 0 775 470 A1

(12)

EUROPEAN PATENT APPLICATION

(43) Date of publication:
28.05.1997 Bulletin 1997/22

(51) Int. Cl.⁶: A61F 2/06, A61M 25/00

(21) Application number: 95117923.3

(22) Date of filing: 14.11.1995

(84) Designated Contracting States:
AT BE CH DE DK ES FR GB GR IE IT LI LU MC NL
PT SE
Designated Extension States:
LT LV SI

(72) Inventors:
• Lukic, Goran
8180 Bülach (CH)
• Gianotti, Marc
Wiesendangen (CH)

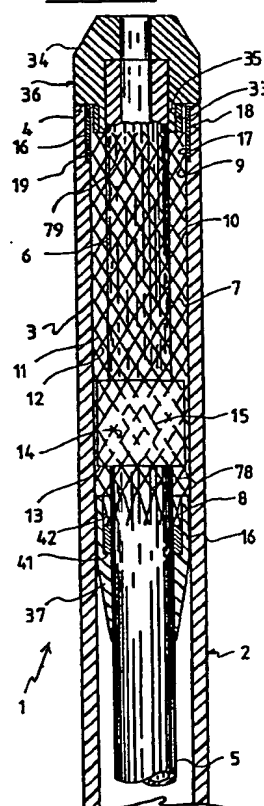
(71) Applicant: SCHNEIDER (EUROPE) AG
CH-8180 Bülach (CH)

(74) Representative: Misrachi, Alfred
15, Ch. de la Plantaz
1024 Ecublens (CH)

(54) Stent delivery device and method for manufacturing a stent delivery device

(57) The stent delivery device comprises an elongated sheath (2) with a self-expandable stent (7) placed in contracted condition within the distal area (3) of the sheath (2). An elongated core (5) is arranged in the sheath (2) for relative longitudinal motion between core and sheath, and drive means (13) are arranged between the core (5) and the stent (7). Scratch protection tubular means (16) comprise a reinforcement ring (18) secured in the sheath (2) and surrounding the distal end portion (79) of the stent when the stent is in contracted condition in the sheath and a tube of thermoformable material (37) heat shrunk over the proximal end portion (78) of the stent and over the core (5).

FIG.1



EP 0 775 470 A1

Description

This invention relates to a stent delivery device comprising an elongated sheath having a distal area with a distal end, a self-expandable stent having proximal and distal end portions with proximal and distal ends and a braided tubular wall, said stent being placed in contracted condition within the distal area of the sheath, elongated core means having proximal and distal areas, said core means arranged in said sheath for relative longitudinal motion between the sheath and core means, and drive means between the distal area of the core means and the self-expandable stent, whereby relative longitudinal motion between said sheath and core means results into longitudinal relative motion between said stent and sheath so as to cause radial self-expansion of at least a longitudinal portion of the stent out of the distal area of the sheath or radial contraction of at least a longitudinal portion of the stent into the distal area of the sheath.

A stent delivery device of that kind is typically shown in the document EP-0596145-A1 of the same applicant as that of the present invention.

The invention also relates to a method for manufacturing a stent delivery device.

Use of self-expandable stents is current for damaged areas or stenoses of body vessels such as food or air pipes, for support, dilatation, repair or bridging such areas.

Where such stents are for use in blood vessels, the stent delivery device must have, i.e., a very small radial size in order to be capable to reach narrow and/or tortuous areas of such blood vessels. Furthermore, the requirements for use in blood vessels are extremely tough in terms of integrity of the stent delivery device because particles of the device getting loose and wandering through the blood vessel may cause complications such as thrombosis. On the other hand, self-expandable stents are most commonly those formed of a braiding composed, for example, of a first plurality of parallel stainless steel spring wires helically wound in a first direction crossing a second plurality of parallel stainless steel spring wires helically wound in a second direction opposite to the first one. The braiding is made in a continuous process and the braided material is then cut in lengths each of which will be used to constitute a stent. As the wires composing the braiding are cut, their ends constitute a plurality of sharp edges. Such edges may dangerously scratch and even perforate the sheath upon passage of the stent therethrough for expansion into the body vessel. Such perforations of the sheath may cause particles of the sheath getting loose and wandering into the vessel. In case of a blood vessel, there may be therefore complications such as thrombosis. This scratch and perforation problem is particularly acute at the distal end of the sheath where the stent exits from the sheath to self-expand into the vessel because rubbing at that place is maximal due to the interaction of a very small surface of contact between

stent and sheath and of the high radial forces generated by the expanding stent against the sheath. However, this problem of scratching and perforation of the sheath also exists for the proximal end of the stent when the latter rubs along the sheath, and possibly exits from the sheath as is the case for a permanently implanted stent. And the problem repeats at both ends of the stent when the stent is successively partly expanded out of the sheath and retracted into the sheath for precise positioning purposes in the required area of the vessel.

Accordingly, there may be a contradictory requirement between small radial size for the stent delivery device to adequately perform in blood vessels and high strength scratch and perforation resistance for the sheath.

It is an object of the invention to provide a stent delivery device that reduces the aforesaid problems and drawbacks, yet allowing a small radial size for the sheath to be performant and safe, particularly for use in blood vessels. It is a further object of the invention to provide a stent delivery device which is economical by the simplicity of its manufacture.

To this effect, the invention complies with the definitions given in the claims.

Accordingly, where the stent delivery device comprises scratch protection tubular means of biocompatible material having an inner wall surrounding at least an end portion of the stent when the latter is in contracted condition in the distal area of the sheath, the risk is reduced of a scratching and/or perforation of the sheath by the distal and/or proximal cutting ends of the stent upon operation thereof through the sheath for self-expansion into a body vessel, and more particularly into a blood vessel where wandering of particles resulting from scratching or perforation of the sheath may be dangerous for the patient. And simultaneously, the sheath may be thin walled as the scratching and perforation resistance is achieved by the scratch protection tubular means. The sheath may be therefore extremely thin, thereby allowing a small radial size for the stent delivery device to efficiently and safely perform through narrow areas such as blood vessels. The scratch protection tubular means do not require complicated or costly structure for the sheath to fully and safely perform anti-scratching and anti-perforation functions. The stent may be repeatedly extracted from and re-inserted into the sheath with a reduced risk for the sheath to release dangerous particles into the blood vessel. And in case of emergency, the doctor may act very rapidly to position the stent even if such a positioning requires repeated extraction of the stent out of the sheath. The doctor may thus concentrate on other major problems without having to slow his action for taking care to avoid potentially trouble causing irregular motions for extracting the stent from the sheath.

The scratch protection tubular means may comprise reinforcement tubular means secured at least in the proximal vicinity of the distal end of the distal area of the sheath. This takes care of the scratch and perfora-

tion problem in a critical location of the sheath when rubbing between stent and sheath is particularly important due to the small surface of contact between stent and sheath and high radial forces due to expansion of the stent. The distal end of the sheath is fully protected and may be safely operated through the vessel.

Where the reinforcement tubular means are formed by a reinforcement ring surrounding at least the distal end of the stent when the stent is in contracted condition in the distal area of the sheath, a very simple protection structure is achieved which may be incorporated in and fastened to the sheath at low cost. And when this reinforcement ring has a rectangular cross-section, a relatively long reinforcement surface is obtained in the proximal vicinity of the distal end of the sheath in combination with low radial place consumption.

The reinforcement tubular means may comprise an outer surface embedded in the sheath to achieve simple and efficient assembly of the reinforcement tubular means to the sheath. In a preferred embodiment, the reinforcement tubular means are embedded in a multilayer structure of the sheath to efficiently match the requirements of a safe assembly between sheath and reinforcement tubular means and to simultaneously allow a choice of materials providing a very low friction for the whole stent along the inner wall of the sheath to thereby reduce rubbing in that area and facilitate relative motion between stent and sheath while retaining a low profile for the sheath wall. In a still preferred embodiment, the multilayer structure is heat shrunk on the reinforcement tubular means to intimately mate the tubular means and sheath.

The reinforcement tubular means may be made of metal to offer the strongest resistance to scratching and/or perforation without interfering on the materials used for making the stent. A metallic reinforcement tubular means may also be extremely thin without losing its resistance to scratching and perforation, which still adds to the profile reduction of the sheath.

In a further embodiment, the reinforcement tubular means are made of a radiopaque metal. In conjunction with a radiopaque marker, for instance conventionally located on the core means at the proximal end of the stent, this radiopaque reinforcement tubular means provide a fixed reference allowing precise knowledge of the percentage of stent which is out of the sheath. Such a percentage knowledge also helps avoiding exaggerated retraction of the stent into the sheath and the resulting potential of damage to the stent or sheath.

In a still further embodiment, the core means extend through the stent and a distal ring of radiopaque material is mounted on the core means within the reinforcement tubular means of radiopaque metal. This allows direct control of the relative position of the stent with respect to the sheath when the stent is retracted into the sheath. Accordingly, it is thereby possible to easily avoid exaggerated retraction of the stent in the sheath and potential damage to the stent or sheath. This may be of great help for the doctor when he has to

rapidly withdraw the stent into the sheath for re-positioning purposes.

Within the frame of the aforesaid distal ring of radiopaque material mounted on the core means within the reinforcement tubular means, the device may advantageously comprise tip means ending the distal area of the core means concentrically to the distal ring of radiopaque material and reinforcement tubular means of radiopaque metal. In addition to the usual advantages of a tip configuration for a smooth insertion of the stent delivery system into the body vessel, the coaxial mounting of the tip on the distal ring of radiopaque material and reinforcement tubular means assures a centering of the tip means on the sheath thereby preventing bending or angle making between the tip and sheath and the potential risk of catching and wounding the body vessel in particular in tortuous areas thereof. Hence, the reinforcement tubular means have a positioning or centering function in addition to the anti-scratching, anti-perforation, and control functions. Within this frame, the reinforcement tubular means may have a first outer diameter whereas the tip means have a second outer diameter greater than the first outer diameter. This configuration acts as an extra safety in case of the unexpected (and even highly improbable) escape of the reinforcement tubular means out of the end area of the sheath. In such a case, the larger diameter of the tip means prevents any passage of the reinforcement tubular means distally beyond the tip means and assures recovery of the reinforcement tubular means out of the body vessel.

When the scratch protection tubular means comprise coverage tube means secured to the proximal end portion of the stent and to the core means, a safety is obtained along the distal area of the sheath against the risk of having sheath particles getting loose from the sheath because of rubbing between the proximal end of the stent and the sheath. When combined to the reinforcement tubular means as described hereinbefore, the resulting configuration of the scratch protection tubular means assures full protection of the distal area of the sheath by the maximal reduction of the risk of having particles of the sheath getting loose from the sheath due to the rubbing between stent and sheath.

Where the coverage tube means are formed by a tube of thermoformable material heat shrunk over the proximal end portion of the stent and over the core means, the tube heat shrunk over the proximal end portion of the stent acts as an assembly help for the manufacturing of the stent delivery device. Such an assembly help disposes of using a special tool to very tightly contract the proximal end portion of the stent for inserting the stent into the sheath and avoiding damage to the sheath. And furthermore, the shrunk tube also acts as a protection against kinking of the sheath proximally of the stent because it somewhat fills the room between the proximal end of the stent and the sheath and also reduces continuously the flexibility of the stent at its proximal end portion.

Where the heat shrunk tube comprises longitudinal cuts extending along a distal portion thereof, the heat shrunk tube may easily separate from the proximal end portion of the stent upon expansion thereof out of the sheath, thereby allowing full expansion and release of the stent out of the sheath for permanent implantation thereof.

Within these configurations, a proximal ring of radiopaque material may be mounted on the core means in the immediate proximal vicinity of the proximal end of the stent, said ring of radiopaque material being embedded in the shrunk tube. This arrangement provides for an easy positioning and fastening for a proximal ring of radiopaque material while assuring a smooth transition between the stent and radiopaque ring which also contributes to reduce the kinking potential of the sheath in that area.

According to a method of manufacturing a stent delivery device to incorporate in a simple and efficient way a reinforcement ring as hereinbefore described, there is provided for engaging on a mandrel a reinforcement ring having a proximal end, a distal end, and a first outer diameter, engaging on the mandrel and proximally of the proximal end of the reinforcement ring a first tube of thermoformable material having a second outer diameter greater than said first outer diameter, engaging on the reinforcement ring a second tube of thermoformable material having a third outer diameter substantially equal to said second outer diameter of the first tube of thermoformable material, engaging on the first and second tubes of thermoformable material a third tube of thermoformable material, heat shrinking said third tube of thermoformable material over said first and second tubes of thermoformable material and reinforcement ring, withdrawing the mandrel out of the reinforcement ring and first tube of thermoformable material, and taking off unwanted surplus portions of the heat shrunk material at the distal end of the reinforcement ring.

These and other objects, features and advantages of the invention will become readily apparent from the following detailed description with reference to the accompanying drawings which show, diagrammatically and by way of example only, preferred but still illustrative embodiments of the invention.

Figure 1 is a side view partly cut of a device in accordance with the present invention with the stent shown in contracted condition in the sheath.

Figure 2 is a side view similar to that of Figure 1, however, with the stent shown partly expanded out of the sheath.

Figures 3 and 4 illustrate a method of manufacturing a stent delivery device in accordance with the invention.

Figure 5 is a side view partly cut of a detail of Figure

1.

Figure 6 is a perspective view illustrating the function of the detail of Figure 5.

The stent delivery device 1 shown in Figures 1 and 2 comprises an elongated sheath 2 having a distal area 3 with a distal end 4. The sheath 2 has a proximal area (not shown) adapted to be connected to a conventional T-connector (not shown) for manipulation and contrast fluid supply purposes. Of course, the sheath 2 is made of a biocompatible material.

Within the sheath 2 is arranged an elongated core 5, for example tubular, having a proximal area (not shown) and a distal area (6). The proximal area of the core 5 is adapted to be connected to a conventional luer lock assembly (not shown) for handling purposes. The core 5 is arranged in the sheath 2 for relative longitudinal movement between the sheath and the core. The core is also made of a biocompatible material.

A self-expandable stent 7 having proximal and distal end portions 78 and 79 with a proximal end 8 and a distal end 9 is mounted on the core 7, within the sheath 2 where it is placed in radially contracted condition within the distal area 3 of the sheath 2. The stent 7 has a braided tubular wall 10 which is conventionally composed of a first plurality of parallel stainless steel spring wires 11 helically wound in a first direction crossing a second plurality of parallel stainless steel spring wires 12 helically wound in a second direction opposite to the first one. Such a braided structure allows radial contraction of the stent when it is placed in the sheath 2 as shown in Figure 1 and radial self-expansion of the stent when it is taken out of the sheath 2 as shown in Figure 2. This configuration is well known in the art and needs no further description. Of course, other known braidings providing the same effect may be used.

Drive means 13 are provided between the distal area 6 of the core 5 and the self-expandable stent 7. In the example shown, these drive means comprise a pad 14 of soft material which mates with the pits and bosses of the braided tubular wall 10 as depicted at 15 in Figure 1. Such a configuration and the method for obtaining it are described in the document EP 0596145A1 which is incorporated hereto by reference. By this arrangement, relative longitudinal motion between the sheath 2 and the core 5 results into longitudinal relative motion between the stent 7 and the sheath 2 so as to cause radial self-expansion of at least a longitudinal portion of the stent 7 out of the distal area 3 of the sheath 2 in a body vessel 20, as shown in Figure 2, or radial contraction of at least a longitudinal portion of the stent 7 into the distal area 3 of the sheath 2, as shown in Figure 1.

Scratch protection tubular means 16 of biocompatible material are arranged in the distal area 3 of the sheath 2 so as to have an inner wall 17 surrounding the distal end portion 79 of the stent 7 when the latter is in contracted condition in the distal area 3 of the sheath 2. Such scratch protection tubular means 16 comprise

reinforcement tubular means 18 which are secured in the proximal vicinity of the distal end 4 of the distal area 3 of the sheath 2. In the example shown in Figures 1 and 2, such reinforcement tubular means 18 are formed by a reinforcement ring which surrounds the distal end portion 79 of the stent 7 when the latter is in contracted condition in the distal area of the sheath 2. Preferably, the ring 18 has a rectangular cross-section and it comprises an outer surface 19 embedded in the sheath 2.

In the embodiment shown in the drawings, the ring 18 is made of metal, preferably a radiopaque metal.

The reinforcement ring 18 may be embedded in a multilayer structure 21 of the sheath 2 and this multilayer structure of the sheath may be heat shrunk on the reinforcement ring 18.

Figures 3 and 4 illustrate a method for manufacturing such a configuration. A reinforcement ring 18 having a proximal end 22, a distal end 23, and an outer diameter 24 is engaged on a mandrel 25. A first tube of biocompatible thermoformable material 26 is engaged on the mandrel 25, proximally of the proximal end 22 of ring 18, which first tube has an outer diameter 27 greater than the outer diameter 24 of ring 18. A second tube of biocompatible thermoformable material 28 is engaged on the reinforcement ring 18, which tube has an outer diameter 29 substantially equal to the outer diameter 27 of the first tube 26. The tubes 26 and 28 have thus their outer surfaces substantially aligned. A third tube 30 of thermoformable biocompatible material is engaged on the first and second tubes 26 and 28 and said third tube is heat shrunk over the first and second tubes 26 and 28 and the reinforcement ring 18 as depicted as 31 in Figure 4. The mandrel 25 is then withdrawn out of the reinforcement ring 18 and first tube 26 and the unwanted surplus portions 32 of the heat shrunk material at the distal end 23 of the reinforcement ring 18 is taken off. By this method, a smooth regular embedding is obtained for the ring in the sheath, avoiding any gaps between the sheath and the ring.

As shown in Figure 1, the core 5 extends through the stent 7 and a distal ring 33 of radiopaque material is mounted on the core within the reinforcement ring 18. A tip 34 ends the distal area 6 of the core 5 concentrically to the distal ring of radiopaque material 33 and to the reinforcement ring 18 and, to this effect, the tip 34 comprises a proximal tubular shoulder 35 on which is mounted the radiopaque ring 33. The tip 34 has an outer diameter 36 which is greater than the outer diameter 24 of ring 18.

As shown in Figures 1 and 2 and in more detail in Figures 5 and 6 scratch protection tubular means 16 are also arranged in the distal area 3 of the sheath 2 so as to have an inner wall 42 surrounding the proximal end portion 78 of the stent 7 when the latter is in contracted condition in the distal area 3 of the sheath 2. Such scratch protection tubular means 16 comprise coverage tube means 37 secured to the proximal end portion 78 of the stent 7 and to the core 5. In the example shown, such coverage tube means are formed by a tube of ther-

moformable material heat shrunk over the proximal end portion 78 of the stent 7 and over the core 5. This tube 37 comprises longitudinal cuts 38 extending along a distal portion 39 of the tube 37. These cuts 38 are forming in the tube a plurality of successive tongues 40. As best seen on Figure 6, these tongues may deploy like flower petals under the radial force exerted by expansion of the stent 7 out of the sheath 2 whereby the tube 37 may easily separate from the proximal end portion of the stent.

A proximal ring 41 of radiopaque material is mounted on the core 5 in the immediate proximal vicinity of the proximal end 8 of the stent 7. This ring 41 of radiopaque material is embedded in the tube 37 which is heat shrunk over the proximal end of the stent and over the core.

Variants are available without departing from the scope of the invention.

For example, the ring 18 may be affixed to the sheath otherwise than by heat shrinking of a structure of the sheath. It may comprise peripheral studs or indentations partly or totally penetrating corresponding recesses provided for in the sheath 2. It may also be affixed to the sheath by means of an appropriate adhesive.

The core 5 may be devoid of a tip such as tip 34.

When the stent is not for permanent implantation in the body vessel, the heat shrunk tube 37 may be replaced by a mere, for instance adhesive, surrounding assembly of the proximal end of the stent to the core.

The drive means 13 may be replaced by any other conventional drive between the core and the stent.

The scratch protection tubular means 16 or ring 18 may extend proximally until the proximal end portion of the stent 7 when the latter is in contracted condition in the distal area 3 of sheath 2. With such an arrangement, the tubular means may also be made of metal, preferably of a radiopaque metal, and assembly thereof to the sheath may be as described for the ring 18. Such a configuration may dispose of using the heat shrunk proximal tube 37 as a sheath protection at the level of the proximal end portion of the stent and as an assembly help for insertion of the stent into the sheath. This extended tubular means may also be secured in the sheath as described for the ring 18.

Claims

1. A stent delivery device (1) comprising an elongated sheath (2) having a distal area (3) with a distal end (4), a self-expandable stent (7) having proximal and distal end portions (78, 79) with proximal and distal ends (8; 9) and a braided tubular wall (10), said stent being placed in contracted condition within the distal area of the sheath, elongated core means (5) having proximal and distal areas, said core means arranged in said sheath for relative longitudinal motion between the sheath and core means, and drive means (13) between the distal area (6) of the

core means (5) and the self-expandable stent (7), whereby relative longitudinal motion between said sheath and core means results into longitudinal relative motion between said stent and sheath so as to cause radial self-expansion of at least a longitudinal portion of the stent out of the distal area of the sheath or radial contraction of at least a longitudinal portion of the stent into the distal area of the sheath, characterized in that it comprises scratch protection tubular means (16, 18, 37) of biocompatible material having an inner wall (17, 42) surrounding at least an end portion (78, 79) of the stent (7) when the stent is in contracted condition in the distal area (3) of the sheath (2).

2. A device according to claim 1, wherein said scratch protection tubular means (16) comprise reinforcement tubular means (18) secured at least in the proximal vicinity of the distal end (4) of the distal area (3) of the sheath (2).
3. A device according to claim 2, wherein the reinforcement tubular means are formed by a reinforcement ring (18) surrounding at least the distal end portion (79) of the stent (7) when the stent is in contracted condition in the distal area (3) of the sheath (2).
4. A device according to claim 3, wherein the reinforcement ring (18) has a rectangular cross-section.
5. A device according to any of claims 2 to 4, wherein the reinforcement tubular means (18) comprise an outer surface (19) embedded in the sheath (2).
6. A device according to claim 5, wherein the reinforcement tubular means (18) are embedded in a multilayer structure (21) of the sheath (2).
7. A device according to claim 6, wherein said multilayer structure (21) is heat shrunk on the reinforcement tubular means (18).
8. A device according to any of claims 2 to 7, wherein the reinforcement tubular means (18) are made of metal.
9. A device according to claim 8, wherein the reinforcement tubular means (18) are made of radiopaque metal.
10. A device according to claim 9, wherein the core means (5) extend through the stent (7), and wherein a distal ring (33) of radiopaque material is mounted on the core means (5) within the reinforcement tubular means (18) of radiopaque metal.
11. A device according to claim 10, further comprising

tip means (34) ending the distal area (6) of the core means (5) concentrically to the distal ring (33) of radiopaque material and to the reinforcement tubular means (18) of radiopaque metal.

12. A device according to claim 11, wherein said reinforcement tubular means (18) have a first outer diameter (24) and the tip means (34) have a second outer diameter (36) greater than said first outer diameter (24).
13. A device according to any preceding claim, wherein said scratch protection tubular means (16) comprise coverage tube means (37) secured to the proximal end portion (78) of the stent (7) and to the core means (5).
14. A device according to claim 13, wherein the coverage tube means are formed by a tube (37) of thermoformable material heat shrunk over the proximal end portion (78) of the stent (7) and over the core means (5).
15. A device according to claim 14, wherein the heat shrunk tube (37) of thermoformable material comprises longitudinal cuts (38) extending along a distal portion (39) thereof.
16. A device according to claim 14 or 15, further comprising a proximal ring (41) of radiopaque material mounted on the core means (5) in the immediate proximal vicinity of the proximal end (8) of the stent (7), said ring of radiopaque material being embedded in the shrunk tube (37).
17. A method for manufacturing a stent delivery device comprising the steps of :
 - engaging on a mandrel (25) a reinforcement ring (18) having a proximal end (22), a distal end (23), and a first outer diameter (24);
 - engaging on the mandrel (25) and proximally of the proximal end (22) of the reinforcement ring (18) a first tube (26) of thermoformable material having a second outer diameter (27) greater than said first outer diameter (24);
 - engaging on the reinforcement ring (18) a second tube (28) of thermoformable material having a third outer diameter (29) substantially equal to said second outer diameter (27) of the first tube (26) of thermoformable material;
 - engaging on the first and second tubes (26, 28) of thermoformable material a third tube (30) of thermoformable material;
 - heat shrinking said third tube (30) of thermoformable material;

mable material over said first and second tubes (26, 28) of thermoformable material and reinforcement ring (18);

- withdrawing the mandrel (25) out of the reinforcement ring (18) and first tube (26) of thermoformable material; and, 5
- taking off unwanted surplus portions (32) of the heat shrunk material at the distal end (23) of the reinforcement ring (18). 10

15

20

25

30

35

40

45

50

55

FIG.1

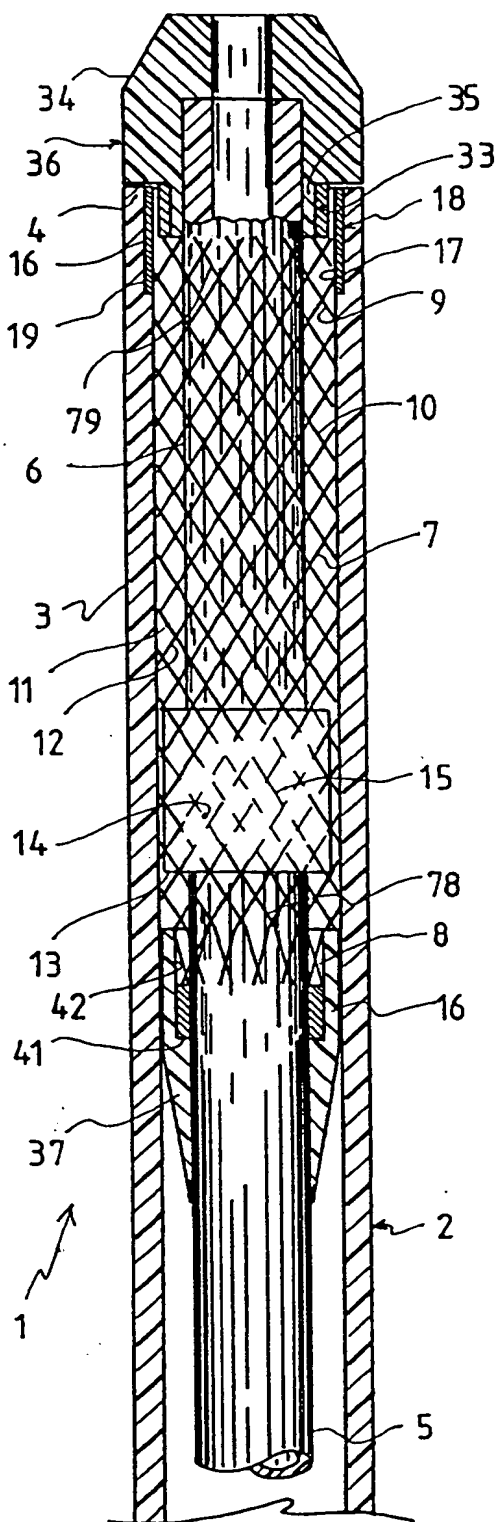
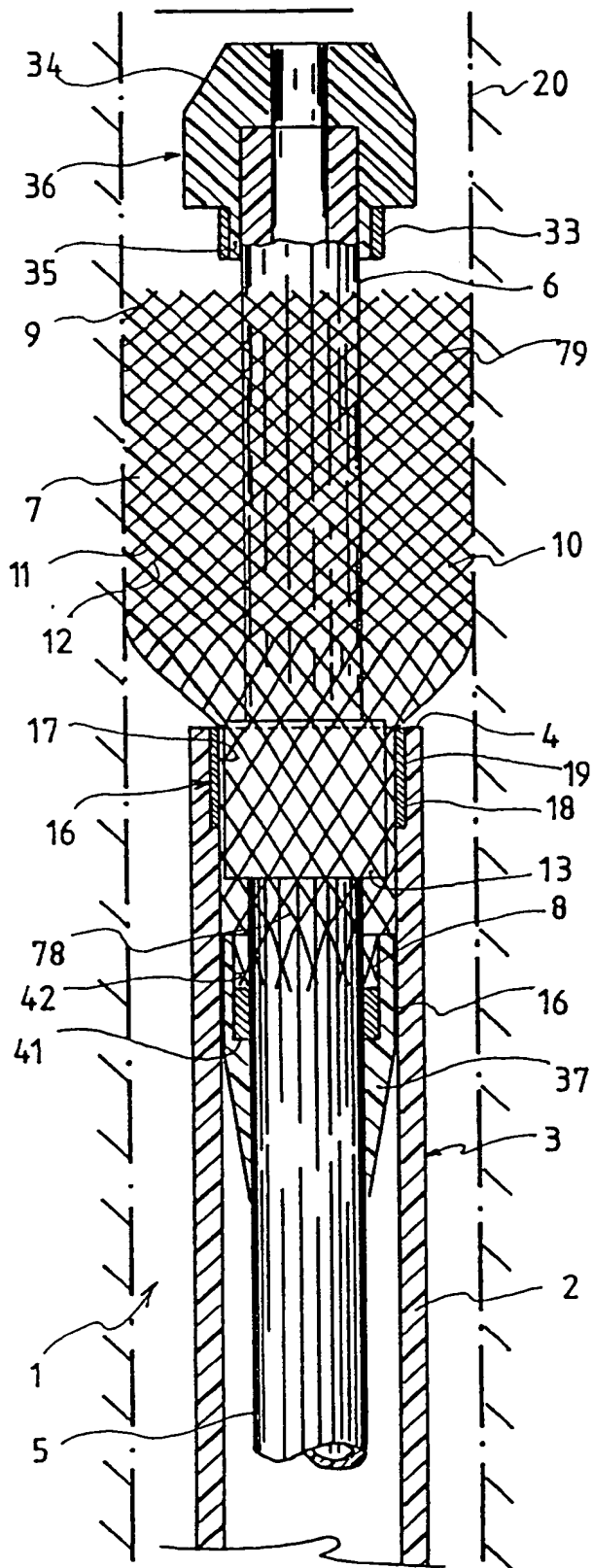
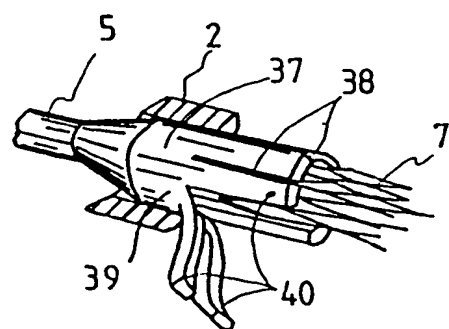
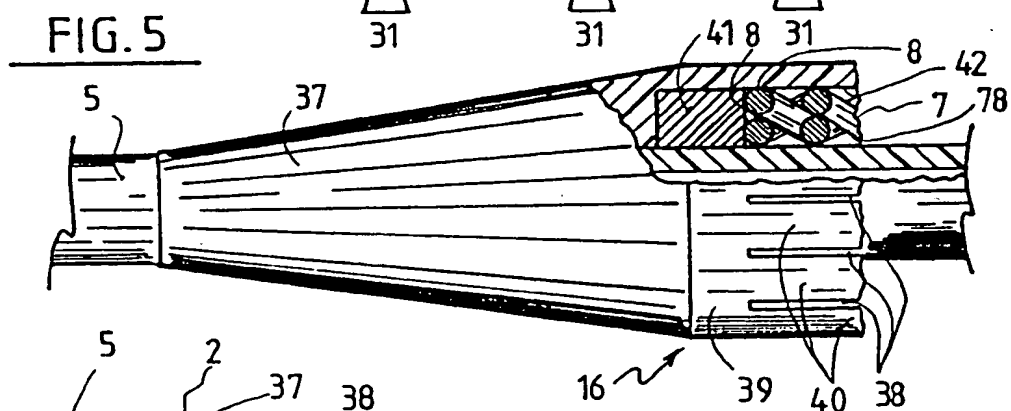
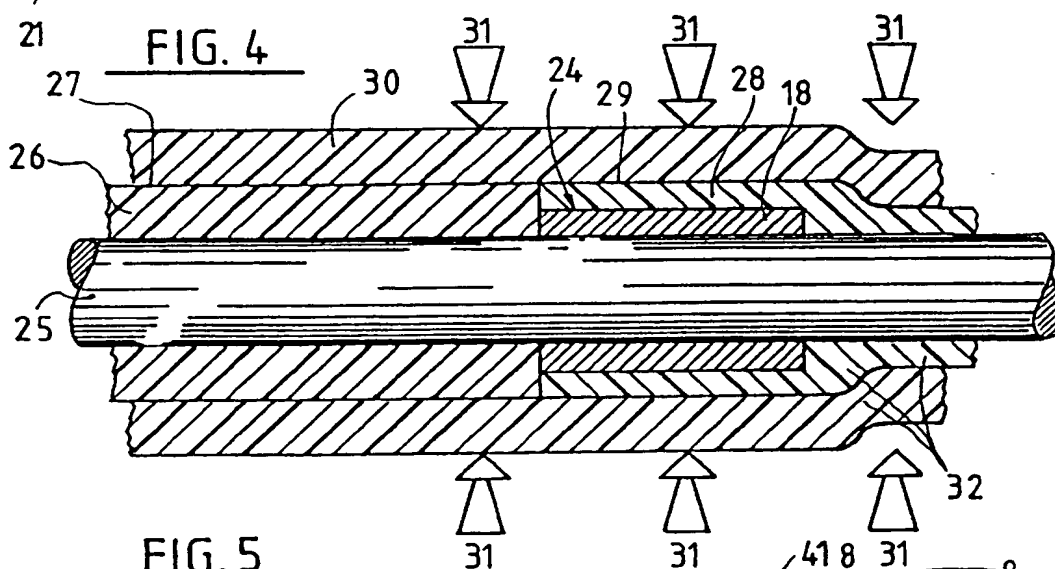
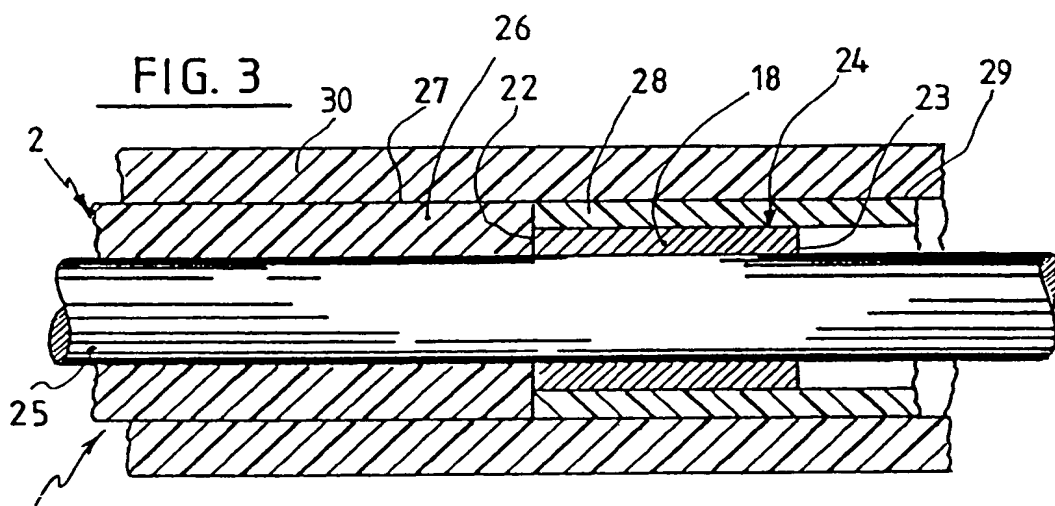


FIG.2







European Patent
Office

EUROPEAN SEARCH REPORT

Application Number
EP 95 11 7923

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.6)
X	EP-A-0 627 201 (SCHNEIDER) * column 4, line 37 - column 5, line 15; figures *	1	A61F2/06 A61M25/00
A	EP-A-0 442 657 (RYAN) * abstract; figures *	1,13	
A	EP-A-0 364 420 (MEDINVENT)		
A	WO-A-90 05554 (BOSTON SCIENTIFIC CORPORATION)		
A	WO-A-93 17636 (LABORATOIRE PEROUSE IMPLANT)		
A	US-A-3 861 972 (GLOVER)		
			TECHNICAL FIELDS SEARCHED (Int.Cl.6)
			A61F A61M
The present search report has been drawn up for all claims			
Place of search THE HAGUE		Date of completion of the search 19 April 1996	Examiner Steenbakker, J
<p>CATEGORY OF CITED DOCUMENTS</p> <p>X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document</p> <p>T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons @ : member of the same patent family, corresponding document</p>			

EPO FORM 1503 (01.92) (P04001)